

OPTICAL SYSTEM FOR A FUNDUS CAMERA

[0001] The invention is directed to an optical system for a fundus camera which serves to image the ocular fundus. When imaging the ocular fundus with a camera of this type, flare generally results at the cornea and at surfaces of the optical system and has a degrading effect on the image quality.

[0002] In its basic construction, a fundus camera comprises a multiple-stage optical system. An ophthalmoscope lens generates an intermediate image that is imaged by a sequential system (principal objective) on a film or a CCD matrix. The ophthalmoscope lens is also a component part of the illumination.

[0003] A particular problem in observing and photographing the fundus is posed by flare at the cornea and at the surfaces of the ophthalmoscope lens because the light which is reflected by the retina and which carries the relevant image information is substantially less intense than the light that is reflected before entering the eye. Troublesome corneal flare is normally prevented by dividing the pupil of the eye. For this purpose, the ophthalmoscope lens images an illumination ring in the pupil of the eye. The illumination rays reflected at the cornea miss the observation aperture. Only the area within the illumination ring is used for observation.

[0004] There are substantially two known concepts for suppressing flare at the ophthalmoscope lens.

[0005] DE-OS 35 19 442 describes an optical system in which components of light that could enter the observation aperture by reflection at the ophthalmoscope lens or cornea are masked out by "black-dot plates" which are arranged at a suitable location in the beam path and which are coated in a defined manner with light-absorbing layers. This method of suppressing reflections has come to be known as "anti-flare dot objective".

[0006] The proximity of the anti-flare dot to the field diaphragm is a disadvantage in this design. The absorption of individual light components can become visible as an inhomogeneous illumination of the ocular fundus. Ring-shaped shadows occur which degrade the image and accordingly impede evaluation by the ophthalmologist.

[0007] Another solution is described in US 4,730,910. This solution does away with masking of determined light components within the illumination optics. Instead of the ophthalmoscope lens, a multiple-lens objective is used whose lenses are tilted relative to one another in such a way that the direct flares at the glass-air interfaces do not enter the observation aperture. For this purpose, the optical axes of the lenses lie in a plane together with the optical axis of the observation beam path. This solution requires a considerable expenditure on mechanical mounting and has considerable problems with correcting imaging errors.

[0008] A system of the type mentioned above exhibits a clear difference between imaging scales in the meridional and sagittal section. Anamorphic effects can be observed in object imaging as well as in pupil imaging (illumination). The images are distorted and there is no similarity of imaging. Further, the system exhibits coma and astigmatism when imaging the axial point and the imaging errors in the field are not symmetric with respect to rotation.

[0009] It is the object of the invention to overcome the disadvantages of the prior art and to provide an optical system for a fundus camera which effectively eliminates flare at the optical surfaces from the imaging beam path and ensures extensive imaging fidelity.

[0010] This object is met by an optical system according to the main claim. Advantageous further developments are described in the subclaims.

[0011] The tilting of the lenses in two planes extending perpendicular to one another brings about matching of the imaging scales for two sections extending perpendicular to one another. The images are less distorted and similarity of imaging is achieved. Further, the axial astigmatism can be corrected in this way and the rotational symmetry of the errors in the field can be reproduced approximately.

[0012] A preferred further development of the invention comprises four collecting lenses which are divided into two lens pairs. The lenses of the first lens pair are tilted in a first plane. The lenses of the second lens pair are tilted in a second plane, these two planes extending perpendicular to one another. It is particularly advantageous when the tilting angle and displacements of the lenses are selected in such a way that the area in the vicinity of the optical axes of the lenses is not penetrated by the illuminating bundle.

[0013] This system enables very good matching of the imaging scales for two sections extending perpendicular to one another.

[0014] The invention will be described more fully in the following with reference to the drawings.

[0015] Fig. 1 shows a side view of the optical system according to the invention;

[0016] Fig. 2 shows a top view of the optical system according to the invention;

[0017] Fig. 3 is a schematic view of the residual distortion.

[0018] Fig. 1 is a schematic side view showing the optical system according to the invention, wherein parts that are not substantial to the invention, such as the patient's eye, light sources, photographic device and observation system, are not shown for the sake of simplicity.

[0019] Four lenses 1, 2, 3, 4 are so arranged along the optical axis 5 that defines the illumination beam path and imaging beam path of the fundus camera that the lenses 1 and 2 are tilted relative to the drawing plane 6 of Fig. 1, while lenses 3 and 4 are tilted relative to the optical axis 5 within the drawing plane 6 so that their optical axes 7 and 8 likewise lie in the drawing plane 6.

[0020] Fig. 2 shows a top view of the optical system. The drawing plane 9 is accordingly perpendicular to the drawing plane 6 of Fig. 1. The lenses 1 and 2 are tilted within the drawing plane 9 such that their optical axes 10 and 11 lie in the drawing plane 9. The lenses 3 and 4 are accordingly tilted relative to the drawing plane 9.

[0021] The lenses are arranged in such a way that the illumination bundle of the imaging beam path and illumination beam path with the optical axis 5 penetrates none of the lenses 1, 2, 3, 4 in their central area, that is, the optical axes 10, 11, 7, 8 of the lenses 1, 2, 3, 4 lie outside the bundle beams shown schematically in Figs. 1 and 2.

[0022] The optical data of a preferred realization of the invention are listed in the following table. Designations with the suffix v pertain to the front sides of the lenses 1, 2, 3, 4 and designations with suffix h pertain to the back sides of the lenses 1, 2, 3, 4.

<i>No.</i>	<i>Radius of curvature [mm]</i>	<i>Distance to the next surface [mm]</i>	<i>Medium following the surface</i>
<i>Obj.</i>	infinity	39.42477	air
<i>1v</i>	-76.12524	16.63675	LaK8
<i>1h</i>	-50.66730	-2.16757	air
<i>2v</i>	-197.58358	29.93724	LaK8
<i>2h</i>	-89.73436	7.92140	air
<i>3v</i>	580.99844	26.79594	LaK8
<i>3h</i>	-260.25600	-9.88489	air
<i>4v</i>	169.89283	20.11881	LaK8
<i>4h</i>	-1636.24830	32.91953	air
	infinity	145.13560	air

[0023] The following table contains the values for the displacements and tilting of the lenses 1, 2, 3, 4 relative to the optical axis 5 that are necessary for realizing this embodiment example.

Surface No.	Type of decentering	Displacement [mm]		Rotation [°]		Placement of center of rotation in z-direction [mm]
		x-direction	y-direction	around x-axis	around y-axis	
1v	1. Displacement, 2. rotation	10.1400	1.0882	0.000	29.760	-23.8578
1h	1. Displacement, 2. rotation	10.1400	1.0882	0.000	29.760	-40.4946
2v	1. Displacement, 2. rotation	-6.5758	1.0882	0.000	-18.959	-93.6604
2h	1. Displacement, 2. rotation	-6.5758	1.0882	0.000	-18.959	-123.5976
3v	1. Displacement, 2. rotation	15.5328	-34.7519	5.988	0.000	-202.8670
3h	1. Displacement, 2. rotation	15.5328	-34.7519	5.988	0.000	-229.6629
4v	1. Displacement, 2. rotation	15.5328	-82.9383	14.841	0.000	465.0016
4h	1. Displacement, 2. rotation	15.5328	-82.9383	14.841	0.000	444.8823
	1. Displacement, 2. rotation, rotated coordinates also apply for the subsequent surfaces	3.7576	-5.0827	2.447	4.089	0.0000

[0024] The distortions resulting with this system are shown in Fig. 3. It can be seen that the imaging scales extensively correspond in the x-direction and y-direction. The comparison grid (straight lines) has the same extension in the x-direction and y-direction. Therefore, the requirements for similarity of imaging are ensured to a very great extent.

[0025] Further, the optical system according to the invention is characterized in that the errors at the edge of field are distinctly symmetric with respect to rotation. This makes it possible to compensate for these errors through a rotationally symmetric sequential system.

[0026] The following table juxtaposes the essential data of an optical system according to the prior art (US 4,730,910 = system A) and according to the invention (system B).

<i>Pupil Imaging</i>	System A	System B
Length of system [mm]	60	104
Focal length f' [mm]	31.5	57.3
Pupil imaging scale β_{px}	-2.19	-2.5
β_{py}	-2.46	-2.5
Imaging length l'_p [mm]	171.6	304
Working distance [mm]	24.2	38.1
Field angle illumination [°]	23.5	26
Average spot radius (axis) [mm]	0.9974	0.2349
Average spot radius (field) [mm]	1.2532	0.4334
Petzval curvature r_p [mm]	-71.9424	-93.4579
Distortion	2.64%	0.74%
Longitudinal color aberration $s_e-s_{C'}$ [mm]	-3.13	-5.76
Longitudinal color aberration $s_e-s_{F'}$ [mm]	3.08	5.66
<i>Object imaging</i>		
Field angle observation [°]	22.5	25
Average spot radius (axis) [mm]	0.0119	0.0020
Average spot radius (field) [mm]	0.0575	0.0158
Distortion	-13.01%	-9.43%
Longitudinal color aberration $s_e-s_{C'}$ [μm]	-17	-7.6
Longitudinal color aberration $s_e-s_{F'}$ [μm]	18	8.9

[0027] A significant improvement over the prior art is achieved in all of the relevant parameters for imaging quality.

[0028] In the realization according to the invention, it is possible to replace the lenses shown in Figs. 1 and 2 with corresponding lens segments which encompass at least the area of the penetration of the illumination beam path and the imaging beam path.

[0029] The invention is not limited to the embodiment example shown herein. In certain cases, it may also be advantageous when the two tilting planes are not perpendicular to one another.

[0030] In order to improve the optical imaging characteristics, it can be advantageous to provide at least one of the lenses with an aspheric surface. It is also possible to realize the invention by using diffractive optical elements instead of one or more lenses.

[0031] The principle of the invention is also applicable in other fields in which flare must be suppressed at optical surfaces.